

The Hamstring/Quadriceps Ratio is an indicator of function in ACL-deficient, but not in ACL-reconstructed knees

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Abstract

Purpose:

The purpose of this study was to investigate isokinetic, eccentric and isometric hamstring/quadriceps (HQ) ratios in patients before and after ACL reconstruction (ACLR) using bone-patella-tendon grafts and to establish the relationships between HQ ratio and knee function.

Methods:

Forty-four patients (mean age of 26.6 years) underwent isokinetic testing of quadriceps and hamstring muscles before and after ACLR and HQ ratios were calculated. Lysholm, IKDC and Cincinnati Scores were used to assess function. Isokinetic concentric and eccentric peak torque (Nm/kg) was measured at three different speeds: 60, 120 and 180 deg/sec. Isometric strength was tested at 30 and 60 degrees of knee flexion.

Results:

For the isometric tests, the HQ ratio between the involved and non-involved limb was not different for the ACLD knee ($p=0.28$) at 30 degree knee flexion but significant at the 60 degree flexion angle ($p=0.02$) and for the ACLR knees at 30 and 60 degrees ($p=0.02$). For the isokinetic tests, the ratio between involved and non-involved limb was significant for ACL-deficient knees at both 60 ($p=0.039$) and 120 deg/sec ($p=0.05$). There were significant differences between limbs for all speeds in ACLR knees ($p=0.0003-0.01$). For the eccentric tests, the HQ ratio between the involved and non-involved limbs were not significant for both the ACLD ($p=0.19$) and ACLR knees ($p=0.29$) at the speed of 60 deg/sec. At 120 and 180 deg/sec there were significant differences between limbs for both the ACLD ($p=0.02$) and ACLR knees ($p=0.003$). Linear regression did not reveal significant relationships between Cincinnati, Lysholm, and IKDC scores and HQ ratios in the ACLD ($R^2= 0.35$, $p=0.58$;

$R^2=0.34$, $p=0.63$; $R^2=0.38$, $p=0.49$). In contrast, there were significant correlations between the Lysholm and IKDC scores and HQ ratios in the ACLR knees ($R^2=0.84$, $p=0.002$; $R^2=0.86$, $p=0.001$).

Conclusions:

The findings of this study suggest that the HQ ratio in ACLD patients was not a predictor but an indicator of patient perceived knee function following ACLR.

Keywords

Anterior cruciate ligament deficient; muscle strength; knee functionality; anterior cruciate ligament reconstruction; bone patellar tendon; hamstring/quadriceps ratio

Level of evidence

Level IV case series

Introduction

Quadriceps and hamstring muscles apply antagonist forces to the tibia, and play an important role in knee stabilization [1]. The hamstring muscles are considered agonists of the anterior cruciate ligament (ACL) and have a protective function at 15-30 degrees of knee flexion, which is the most common position for an ACL injury [2]. Deficits of hamstring muscle strength in the ACL-deficient knee can be an indicator of poor knee function [3]. Likewise, neurophysiological responses such as quadriceps inhibition can further result in a relatively stronger agonist, facilitating hamstring strength and activation [4-6]. It is well known that strength deficits following ACL injury and reconstruction are common, and influence the balance between the quadriceps and hamstring muscle groups [7-10]. In fact, persistent muscle weakness may cause further alterations in the hamstring-quadriceps ratio (HQ ratio) resulting in dynamic instability, and it may increase the risk of further injury [10,11].

Myer et al. demonstrated decreased hamstring but not quadriceps strength in female athletes following ACL injury compared to non-injured athletes [12]. In ACL reconstructed athletes, HQ ratios remained unbalanced in the affected knee [13]. Hohmann et al. has demonstrated that peak torque strength values of both the quadriceps and hamstring muscles was not a predictor of knee function [14]. However, limb symmetry indices indicated that the HQ ratio might possibly play an important role when considering whether ACL-deficient athletes can cope with knee strength deficits [14]. These findings further support Kannus & Jarvinnen's study which suggested more than 25 years ago that function is related to the ideal HQ ratio, which is the HQ ratio of the contralateral uninvolved limb [15].

The ratio between hamstring and quadriceps torque has been investigated for more than three decades, and the conventional HQ ratio of 0.6, with a range from 0.5 to 0.75, has been

generally accepted as the normative value [7,16,17]. If the HQ ratio is higher the hamstrings have an increased functional capacity to provide stability to the knee which may reduce both anterior translation and anterolateral subluxation [18,19]. Moreover, it has been suggested by various authors that the HQ ratio is a determinant of knee function and could possibly be used as a parameter to monitor rehabilitation and return to sports following ACL injury [1,3,9,10,13,15].

The purpose of this study was to investigate isokinetic concentric, eccentric and isometric HQ ratios at three speeds using an isokinetic dynamometer in patients before and after ACL reconstruction using bone-patella-tendon grafts. The secondary purpose was to investigate the relationships between HQ ratio and knee function.

Methods

Subjects:

For this prospective cohort study volunteers were recruited from the Orthopaedic Sports Injury Clinic. This clinic captures more than 80% of the sporting community in the region with referrals being made through the emergency department, general practitioner, sports physician, physiotherapist, or a direct referral from the various local sporting codes. ACL-deficient patients are usually seen within four weeks of the injury, and referred to the physical therapist for prehabilitation. ACL-deficient patients were recruited if they met the inclusion criteria and were followed-up through this clinic. Ethical clearance was obtained from both the Human Ethics Research Review Panel of the University (Clearance No. 02/09-74) and the Regional Health District (Clearance No. 02/11).

Patients were included if they had an isolated ACL injury, presented to the clinic within 4 weeks of injury, completed a 12-week physical therapy program, underwent surgical reconstruction between four and six months following injury, and were aged between 18 and 50 years. The following exclusion criteria were applied: concomitant injuries to the meniscus, medial and lateral collateral ligaments, posterior cruciate ligament, articular cartilage, or any other injury/fracture to the ipsi- or contralateral lower extremity demonstrated on MR imaging or during the initial arthroscopic examination, and coronal plane deformities of more than 10 degrees either varus or valgus on long leg weight-bearing radiographs. Patients with reported intra- and postoperative complications, additional surgical procedures during follow-up, or patients who had additional surgical procedures such as realignment procedures were also excluded.

Surgical Procedure and Rehabilitation

An arthroscopic assisted ACL-reconstruction with the central third of the patellar tendon and using two interference screws was performed as described previously [20]. Post-operatively, the extremity was placed into a ROM brace for six weeks. Immediate weight-bearing as tolerated by the patient was started from day one post-surgery, and a previously described accelerated rehabilitation protocol was used for all patients [21].

Outcome measures

Knee Scoring Systems

The Cincinnati Knee Rating System (CKRS) is a validated outcome instrument that is specifically applicable to ACL and all 13 scales were used in this study. [22] The senior author (EH) performed both the clinical examination and interpreted the radiographs using the CKRS criteria.

Instability testing using a KT-2000, all functional hopping tests, the subjective assessment, and activity level scores were performed by an independent research associate at the University's Performance Laboratory. For the functional hopping tests (single-leg-hop, timed-hop for distance, and vertical-jump) patients were asked to perform each of the hopping tests until three valid attempts were recorded. Each testing session was conducted with the non-involved leg first, followed by the involved extremity, with results averaged over the three attempts.

The Lysholm score is a patient administered score and was used in this study. [19,23]. The subjective IKDC knee form was used as a patient-oriented questionnaire to assesses symptoms and function of daily living and activities. [24,25]

Muscle strength

Muscle strength was assessed using a BiodexTM Isokinetic Dynamometer (System 3 BIODEXTM, Shirley, New York). Isokinetic concentric/concentric and eccentric/eccentric muscle strength, for both the hamstring and quadriceps muscles, was tested at three different speeds (60,120 and 180 deg/sec), and isometric strength was tested at 30 and 60 degrees of knee flexion for the involved and non-involved limbs. A set of five maximal extension and flexion repetitions were performed at the nominated speeds. Peak torque (Nm/kg) generated by both the quadriceps and hamstring muscles of the involved and non-involved limbs were corrected for bodyweight, and a mean from the three best trials for each test speed and test mode was calculated. For isometric tests, the highest force generated (Nm/kg) during the two knee extension and flexion trials was recorded for subsequent analysis. The HQ ratio was

calculated by dividing the means of the peak torque recorded for the hamstrings and quadriceps, respectively, and was presented in numerical values.

Testing protocol

ACL-deficient patients were treated by a physical therapist for 12 weeks. Treatment included ROM exercises, proprioceptive exercises, and anti-inflammatory measures. Patients were tested once the knee effusion had resolved, and full ROM with good subjective quadriceps control was achieved. This typically occurred within 1-2 weeks following the completion of the physical therapy intervention. ACL-reconstructed subjects were tested between 18 and 24 months following ACL reconstruction surgery.

Following a five-minute warm-up session on a Monark™ Friction-Braked Cycle Ergometer at a power output of 50-100W, the hopping tests were performed as recommended by Barber, et al [22]. The Cincinnati questionnaires as well as the clinical examination were then completed, and the session concluded with the assessment of muscle strength, following a five-minute break between isometric, isokinetic, and eccentric testing to avoid fatigue related errors.

Statistical Analysis

An a-priori sample size calculation was performed. The study was powered to detect a 10% difference between limb HQ ratios using a medium effect size (0.5), alpha level of 0.05 and a power level of 0.8, requiring 27 patients. The relationships between HQ ratios and knee function as assessed by the CKRS, Lysholm and IKDC scores using the above parameters, was able to detect a statistically significant ($p=0.05$) correlation of $r \geq 0.50$ between the HQ

ratio of the involved limb and knee function. The sample size calculation based on these parameters indicated that 37 patients were necessary to achieve 90% statistical power.

Means and standard deviations were calculated for the dependent variables. Data normality was assessed using the Kolmogorov-Smirnov test with Lilliefors corrections. A linear regression model was used to establish the strength of the relationships between the HQ ratios of the involved limbs for all tests, speeds, and knee function as assessed by CKRS, Lysholm, and IKDC scores. The coefficient of correlation “r” was interpreted according to Cohen [26] in the following fashion: 0.0 – 0.3 weak, 0.31–0.5 moderate, >0.51 strong.

A level of significance of $p < 0.05$ was selected in all analyses to limit the chance of Type I error to 5%. HQ ratios between the involved and non-involved limbs were analyzed using a two-tailed paired student t-test. All analyses were conducted using Systat (version 13; Systat, Chicago, IL).

Results

Forty-four ACL-deficient subjects with a mean age of 26.6 years were included in this study. There were 33 males with a mean age of 26.4 (16-49) years and 11 females with a mean age of 27 (17-38) years. The mean follow-up was 28.5 (+4.3) months. The mean Cincinnati score was 62.0 ± 14.5 in the ACL-deficient and 89.3 ± 9.5 in the ACL-reconstructed subjects. The mean Lysholm score was 60.4 ± 19.7 in the ACL-deficient and 91.6 ± 10.1 in the ACL-reconstructed subjects. The mean IKDC score was 53.2 ± 17 in the ACL-deficient and 82.9 ± 9.7 in the ACL-reconstructed subjects.

The HQ ratios for isometric, isokinetic and eccentric muscle strength are shown in tables 1-3. For the isometric tests, the HQ ratio between the involved and non-involved limb was not different for the ACL-deficient knee ($p=0.28$) at 30 degree knee flexion. Significant differences between limbs were observed for the ACL-deficient knees at the 60 degree flexion angle ($p=0.02$) and for the ACL-reconstructed knees at 30 and 60 degrees ($p=0.02$) (Table 1). The HQ ratios decreased following ACL reconstruction for the involved and non-involved limbs between 4.3% and 22.5%. These changes were significant for the isometric test at 30 degrees of knee flexion (Table 1).

Table 1: Hamstring Quadriceps Ratios for Isometrics Strength

Isometric 30		ACLD	ACLR	Difference ACLD-ACLR	P-levels
INV	Mean+SD	0.83+0.37	0.69+0.14	16.9%	0.02
	95% CI	0.77-0.89	0.64-0.74		
NON	Mean+SD	0.80+0.29	0.62+0.12	22.5%	0.0005
	95%CI	0.75-0.85	0.62+0.12		
Difference INV-NON		3.6%	10.2%		
P-levels		0.28	0.02		
		37	92		
Isometric 60		ACLD	ACLR	Difference ACLD-ACLR	P-levels
INV	Mean+SD	0.52+0.22	0.49+0.1	7.7%	0.38
	95% CI	0.44-0.60	0.44-0.54		
NON	Mean+SD	0.46+0.19	0.44+0.12	4.3%	0.13
	95%CI	0.37-0.55	0.48-0.50		
Difference INV-NON		11.5%	10.2%		
P-levels		0.02	0.02		

For the isokinetic tests, the HQ ratio between the involved and non-involved limb was significant for the ACL deficient knees at both 60 ($p=0.039$) and 120 deg/sec ($p=0.05$). There were significant differences between limbs for all speeds in the ACL-reconstructed knees ($p=0.0003-0.01$) (Table 2). The HQ ratios increased between 7.3 and 25.8% for the

involved and non-involved limbs following ACL reconstruction for the tests at both 60 and 120 deg/sec, and was maintained or increased for tests performed at a speed of 180 deg/sec. These changes were only significant at the 120 deg/sec speed ($p=0.02$). (Table 2).

Table 2: Hamstring Quadriceps Ratios for Isokinetic Strength

Isokinetic 60						
		ACLD	ACLR	Difference ACLD-ACLR	<i>P</i> -levels	
INV	Mean+SD	0.50+0.37	0.62+0.21	24%	0.09	
	95% CI	0.38-0.62	0.50-0.72			
NON	Mean+SD	0.41+0.22	0.44+0.11	7.3%	0.48	
	95%CI	0.31-0.51	0.35-0.55			
Difference INV-NON		18%	29%			
<i>P</i> -levels		0.039	0.0003			
Isokinetic 120						
		ACLD	ACLR	Difference ACLD-ACLR	<i>P</i> -levels	
INV	Mean+SD	0.46+0.30	0.62+0.25	25.8%	0.02	
	95% CI	0.37-0.55	0.53-0.64			
NON	Mean+SD	0.36+0.14	0.43+0.12	19.4%	0.04	
	95%CI	0.32-0.40	0.38-0.48			
Difference INV-NON		21.7%	30.6%			
<i>P</i> -levels		0.05	0.0003			
Isokinetic 180						
		ACLD	ACLR	Difference ACLD-ACLR	<i>P</i> -levels	
INV	Mean+SD	0.61+0.07	0.61+0.36	0	0.99	
	95% CI					
NON	Mean+SD	0.68+0.14	0.54+0.29	12.1%	0.53	
	95%CI					
Difference INV-NON		11.5%	11.5%			
<i>P</i> -levels		0.43	0.01			

For the eccentric tests, the HQ ratio between the involved and non-involved limbs were not significant for both the ACL-deficient ($p=0.19$) and ACL-reconstructed knees ($p=0.29$) at the speed of 60 deg/sec. At 120 and 180 deg/sec there were significant differences between limbs

for both the ACL-deficient ($p=0.02$) and ACL-reconstructed knees ($p=0.003$) (Table 3). The HQ ratios increased marginally between 1.7 and 14% for the involved and non-involved limbs following ACL reconstruction for the tests at all speeds, although these changes were not significant (Table 3).

Table 3: Hamstring Quadriceps Ratios for Eccentric Strength

Eccentric 60						
		ACLD	ACLR	Difference ACLD-ACLR	<i>P</i> -levels	
INV	Mean+SD	0.61+0.04	0.64+0.19	4.9%	0.33	
	95% CI	0.60-0.62	0.60-0.68			
NON	Mean+SD	0.67+0.19	0.69+0.15	3%	0.59	
	95%CI	0.62-0.72	0.65-0.73			
Difference INV-NON		9.8%	7.8%			
<i>P</i> -levels		0.02	0.29			
Eccentric 120						
		ACLD	ACLR	Difference ACLD-ACLR	<i>P</i> -levels	
INV	Mean+SD	0.58+0.21	0.62+0.18	6.9%	0.38	
	95% CI	0.55-0.61	0.59-0.65			
NON	Mean+SD	0.64+0.13	0.73+0.2	14%	0.06	
	95%CI	0.60-0.68	0.72-0.74			
Difference INV-NON		10.3%	17.8%			
<i>P</i> -levels		0.02	0.02			
Eccentric 180						
		ACLD	ACLR	Difference ACLD-ACLR	<i>P</i> -levels	
INV	Mean+SD	0.57+0.19	0.58+0.15	1.7%	0.80	
	95% CI					
NON	Mean+SD	0.66+0.13	0.69+0.15	4.5%	0.43	
	95%CI					
Difference INV-NON		15.8%	18.9%			
<i>P</i> -levels		0.003	0.02			

Linear regression did not reveal significant relationships between Cincinnati, Lysholm, and IKDC scores and HQ ratios in the ACL-deficient knees. The R-squared coefficient of

determination was 0.35 (F=0.89, p=0.58) for the Cincinnati score, 0.34 (F=0.84, p=0.63) for the Lysholm score, and 0.38 (F=0.987, p=0.49) for the IKDC score. In contrast, linear regression revealed significant and strong correlations between the Lysholm and IKDC scores and HQ ratios in the ACL-reconstructed knees. The R-squared coefficient of determination was 0.84 (F=4.971, p=0.002) for the Lysholm score and 0.86 (F=5.57, p=0.001) for the IKDC score. There was a non-significant correlation (R-squared 0.633, F=1.62, p=0.18) for the Cincinnati score. Further analysis revealed that these correlations were only significant for all three isokinetic speeds.

Discussion

The most important finding of this study was that HQ ratios did not predict function in the ACL-deficient knees, but were strong predictors of function in the ACL-reconstructed knees. However, in the ACL-reconstructed knees HQ ratio predicted patient perceived subjective knee function, with the Lysholm and IKDC scores as the dependent variables. HQ ratios did not predict knee function with the Cincinnati score. In addition, these correlations were only significant for the isokinetic tests.

A reduction in quadriceps strength in ACL-deficient knees has been observed by many authors [6,8,9,11,14,21,27]. For example, a study by Hohmann et al demonstrated that quadriceps strength deficits do not appear to significantly influence the perception of knee function in ACL-deficient patients [14]. In fact, the results showed that muscle strength was not an important factor in predicting knee function, but that lower limb symmetry indices were [14]. Despite significant differences between limb HQ ratio in ACL-deficient patients, this study could not demonstrate a correlation with knee function. It appears that neural

regulation in the ACL-deficient knees attempts to maintain limb symmetry and a balanced agonist/antagonist ratio to dynamically stabilize unstable joints.

Other studies have suggested that possible reflex and other upper motor neuron controlled mechanisms, including arthrogenic inhibition of both the involved and non-involved limbs, resulted in downregulation of muscle activation, quadriceps/hamstring co-contractions, and feed-forward strategies, ensuring that the HQ ratio remains stable within the normative values [14,28,30]. In the current study, the HQ ratio in the ACL-deficient subjects were certainly within the normative values, and this is perhaps a possible prerequisite to perceive the knee as normal [7,16,17].

If in fact normal HQ ratios are required in ACL-deficient patients to subjectively perceive knee function as normal, even if both quadriceps and hamstring muscle strength is reduced, we speculate that the neuromuscular system must either downregulate the antagonist or upregulate the agonist. We observed an increase in the HQ ratio to following ACL-reconstruction, which could be an indication these mechanisms are regulating muscle strength balance. The inevitable increase in quadriceps strength with rehabilitation should have decreased the HQ ratio, which was not observed in our study cohort. These assumptions are supported by St Clair-Gibson et al., who has shown that HQ ratios were similar and normal in both chronic ACL-deficient patients and uninjured individuals [31]. These authors suggested that muscle co-ordination strategies may have been altered to maintain normal limb activity despite muscle strength losses [31]. Similarly, Lee et al. demonstrated a 50% reduction of thigh muscle strength in a group of patients with a chronic ACL-tear, but they still observed HQ ratios that were comparable to a normal control group [10].

In a recent meta-analysis, Kim et al. reported that ACL-deficient patients experience an uneven reduction in isokinetic strength of the limb muscles resulting, in a slight increase in HQ ratio in ACL-deficient knees [9]. These increases were mainly observed at a 60 degree knee flexion. In contrast to Kim et al, we observed an increase in HQ ratios after the ACL was reconstructed [9]. Kim suggested that higher velocities slightly underestimate hamstring strength because strength is usually measured early after the onset of contraction [9]. One possible explanation for the findings observed in our cohort is that the ACL was reconstructed using a bone-patella-tendon-bone graft, possibly resulting in weakness of the quadriceps muscle. In support of our findings, Zhang et al has previously demonstrated that the HQ ratio was increased when using patella tendon grafts for ACL reconstruction [32].

We also observed significant differences between the groups, using the contralateral uninvolved limb as a control, for all speeds and strength tests, as was suggested by Kannus & Jarvinnen [15]. The HQ ratios were higher for almost all velocities and contraction types, although marked systematic variability was observed and were different between contraction types, with HQ ratios still within the reported normal ranges [7,16,17]. This was not surprising, since these differences have also been reported by other authors [13,18,32].

With surgical reconstruction of the anterior cruciate ligament, static knee stability is restored, and the need to downregulate quadriceps activity reduces with rehabilitation [34,35,36]. In our cohort, the HQ ratio increased following ACL reconstruction clearly favoring the hamstring muscle group, and this was consistent with other studies. Hiemstra et al. demonstrated an increase of the HQ ratio during eccentric contractions for all joint angles and angular velocities [18]. Jordan et al compared HQ ratios in ACL reconstructed elite ski racers and reported that ACL reconstructed athletes had an increased HQ ratio [13]. The authors

speculated that significant quadriceps maximal strength deficit was at least partially responsible for this finding. A major limitation of the Jordan study was both the small sample size and the variety of grafts used.

The mechanisms behind strength balances for knee stability are clearly not yet fully understood, and are open to speculation. However, similar to other neurogenic based responses, reflex pathways and neuro-regulatory systems require afferent input. There are abundant afferent sensory receptors in the periarticular tissues around the knee that constantly feed information to the higher neurons, allowing alteration and regulation of efferent motor output [37,38].

Vairo et al. has shown that both neuromuscular and biomechanical adaptations occur to stabilize the knee. These adaptations include co-contraction of quadriceps and hamstring muscles, greater hamstring muscle activation, and increased hip, knee, and ankle joint flexion angles to reduce the vertical ground reaction forces during landing tasks [39]. In an earlier study, we demonstrated that normal knee symmetry indices in ACL-deficient knees are related to function, whereas in ACL reconstructed knees peak torque values are better correlated with knee function [14]. Interestingly, HQ ratios also play an important role with other knee pathology. For example, Guney et al. demonstrated a significant relationship between the Kujala score and HQ ratios in patients with patella-femoral pain [40]. Müller et al. showed that HQ ratios following autologous chondrocyte implantation (ACI) in the patellofemoral joint are significantly different to those observed in patients who underwent condylar ACI [41]. These consistent patterns of neuromuscular adaptations seem to have evolved to protect the knee from mechanical overloads.

This study has various limitations. The HQ ratios were calculated from the peak torque values at different velocities and contraction types, and these ratios can vary depending on angular velocity and knee flexion angles. To reduce confounders and sampling bias we used strict inclusion and exclusion criteria, resulting in a smaller sample size. However, an a-priori sample size was performed to minimize the probability of type II error. As a result, the external validity of this study is limited, and caution should be exercised before generalizing these results to patients with concomitant injuries such as meniscal tears, other associated ligamentous injuries, or chondral defects.

Conclusion

The findings of this study suggest that the hamstring/quadriceps ratio in ACL-deficient patients was not a predictor of knee function. However, it was an indicator of knee function when using patient-centered subjective outcome scores following ACL-reconstruction. Moreover, the HQ ratios increased for all velocities and contraction types following reconstruction surgery, but those ranges were within normal values for both ACL-deficient and ACL-reconstructed knees.

Compliance with ethical standards

Conflict of interest

The authors declare that they have no conflict of interest.

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Ethical approval

All procedures performed in studies involving human participants were in accordance with the ethical standards of the institutional and/or national research committee and with the 1964 Helsinki declaration and its later amendments or comparable ethical standards.” Informed consent was obtained from all individual participants included in the study.”

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