Carbon Monoxide and Iron Modulate Plasmatic Coagulation in Alzheimer’s disease

Vance G. Nielsen¹*, Etresia Pretorius², Janette Bester², Wayne K. Jacobsen¹, Patrick K. Boyle¹, Joao P. Reinhard¹

¹The Department of Anesthesiology, the University of Arizona College of Medicine, Tucson, Arizona, USA; and the Department of Physiology; ²Faculty of Health Sciences, University of Pretoria, Arcadia, South Africa

Abstract: Alzheimer’s disease (AD) is a significant source of morbidity and mortality for millions of people worldwide, and multiple potential etiologies have been postulated to contribute to AD. Among these, spontaneous cerebral emboli and increased cerebral and circulating heme oxygenase (Hmox) activity in AD patients are of particular interest, as two of the products of Hmox activity, carbon monoxide (CO) and iron enhance plasmatic coagulation and modify the ultrastructure of thrombi. We hypothesized that patients afflicted with AD would have coagulation kinetics modulated by CO and iron. Using viscoelastic assessments of coagulation, it was determined with a small cohort (n=11) of AD patients that all had enhancement of coagulation by CO, iron, or both. In a complementary fashion, it was determined that a separate cohort (n=12) of AD patients had thrombi with ultrastructural features consistent with iron and CO exposure as assessed with scanning electron microscopy. Further, when stratified by normal or abnormally increased serum ferritin concentrations (which can be increased by Hmox), the AD patients with abnormal ferritin concentrations had significantly thinner fibrin fiber diameters, not unlike that noted when normal plasma is mixed with iron or CO. In sum, AD patients were noted to have plasmatic coagulation kinetic and thrombus ultrastructural changes consistent with exposure to CO and iron. Future investigation of CO and iron in the pathogenesis of Alzheimer’s disease is warranted.

Keywords: Alzheimer’s disease, carbon monoxide, iron, heme oxygenase, scanning electron microscopy, thrombelastography.

INTRODUCTION

Alzheimer’s disease (AD) is a major source of morbidity and mortality for millions of people worldwide, and intense investigation has led to multiple etiological constructs contributing to AD [1-12]. In addition to the recently reviewed, original ‘amyloid cascade hypothesis’ [1], the development and progression of AD have been associated with viral infection [2], vascular damage from pulse pressure [3], regional deposition of metals, such as iron, resulting in oxidant injury [4-8], metabolic syndrome and morbid obesity [8-10], and long term exposure to spontaneous cerebral microemboli [11, 12]. Of these various paradigms, the notion that spontaneous emboli, most likely due to systemic hypercoagulability, is of particular interest. AD patients have been documented to have abnormally increased activated Factor VII, von Willebrand factor and prothrombin 1+2 fragment in their circulation [13], the substrate and result of intravascular thrombin generation. Of interest, while patients with AD were noted to have fibrinogen concentrations that on average were not abnormally increased [13], another work noted that patient with mild cognitive impairment were at greater risk of more rapid advancement to AD if their circulating fibrinogen concentration was >300 mg/dl [14]. Further, patients with AD have been noted to have plasma thrombus fibrin polymerization that is structurally similar to iron-exposed plasma [15], and AD patients with abnormally increased ferritin concentrations showed red blood cell morphological changes, with increased membrane stiffness documented with atomic force microscopy [16]. In sum, there is biochemical and ultrastructural evidence of circulating abnormal intravascular thrombin generation, rigid red blood cells, and consequent abnormally appearing fibrin polymerization in thrombi obtained from patients with AD, all of which could contribute to spontaneous emboli.

Given the aforementioned morphological changes in fibrin in plasma obtained from AD patients, it is of particular interest that carbon monoxide [CO] and iron enhance plasmatic coagulation kinetics and modify ultrastructure by modulating fibrinogen [17]. Iron decreases the onset time of coagulation and enhances the speed of clot formation, CO enhances the speed of clot formation and final clot strength, and iron and CO interact kinetically in an additive fashion [17]. Further, both iron and CO act as antifibrinolytic agents when tissue-type plasminogen activator (tPA) is the fibrinolysin [17]. These facts are of importance in the setting of AD, as the endogenous enzyme system responsible for heme catabolism, heme oxygenase (Hmox), has been found to be enhanced in both the brain and circulation of AD
patients [18-21], and Hmox catabolism of heme results in the release of iron and CO [22]. In contrast to the aforementioned data, in a recent review [23] CO has been noted to act as an anti-apoptotic agent that decreases the generation of reactive oxygen species, especially in situations of acute neurological ischemia-reperfusion injury in rodent models. However, inhibition of Hmox in a murine model of AD involving a double transgenic mouse (APP<sub>swed/PS1<sub>E9</sub>) significantly diminished the behavioral deficits and neuropathological changes over time compared to mice not administered a Hmox inhibitor [24]. When all these data are considered as a whole, Hmox enhanced coagulation could play a role in spontaneous thrombus formation not just in the peripheral circulation as documented by previous ultrasonic investigations [11,12], but perhaps more regionally (and intensely) in the microcirculation of the brain itself.

The first goal of this study was to determine if iron and CO enhanced coagulation/diminished fibrinolysis was present in plasma obtained from AD patients using viscoelastic assessments of coagulation and fibrinolytic kinetics as previously described [25-27]. The second goal was to image thrombi obtained from patients with AD with various degrees of iron exposure/inflammation with scanning electron microscopy (SEM), and examine these clots for signs of iron and CO modified fibrin polymer formation [17].

MATERIALS AND METHODS

Viscoelastic Plasma Coagulation and Fibrinolysis Analyses.

All viscoelastic method-based experimentation was completed at the University of Arizona. To establish normal laboratory ranges for the subsequently described assays, human plasma (George King Bio-Medical, Overland Park, KS, USA) anticoagulated with sodium citrate was obtained, which was composed of plasma from 30 individuals (15 males, 15 females; mean age 30 years, with range of 20 years to 47 years). All subjects were confirmed to be disease-free, nonsmokers, and not pregnant.

With regard to AD patient samples, they were obtained from a commercial vendor (PrecisionMed, Inc., Solana Beach, CA, USA). This vendor collects various body fluids (e.g., cerebral spinal fluid, blood) from patients being monitored over time that are diagnosed with minimal cognitive impairment (MCI) or Alzheimer’s disease. The patient centers involved are located throughout the United States, with ethical oversight provided by the Western Institutional Review Board (Puyallup, WA, USA). The protocol number for this particular study was #8009. The AD patients had to meet the following criteria for inclusion: mini mental state exam (MMSE) score ≥14 to ≤28; sign an approved written consent; agree to venipuncture; be ≥50 years of age; have a brain magnetic resonance imaging or computed tomographic study excluding other causes of neurological compromise; Hachinski score ≤4; have a diagnosis of dementia or MCI established by clinical exam and documented by MMSE and other neuropsychological exams. For our specific study, we added the inclusion criteria that the AD patients be nonsmokers, have no congenital bleeding abnormality and were not anticoagulated. After these inclusion criteria were met, whole blood (5 ml) was obtained from a peripheral vein on one of the patients’ arms. The blood sample was anticoagulated with sodium citrate (9 parts blood to 1 part 0.105M sodium citrate), centrifuged at 3000xg for 15 min at room temperature, with plasma removed, aliquoted and placed at -80°C before transport to the University of Arizona. After all plasma samples were collected, they were sent on dry ice and kept at -80°C prior to experimentation.

Coagulation Analyses and Carboxyhemefibrinogen (COHF) Assay

Plasma samples were thawed to 37°C just prior to analysis. Mixture volume for subsequently described samples was 359.4 µl. Samples were composed of 326 µl of plasma; 10 µl of tissue factor (0.1% final concentration in dH2O; Diagnostica Stago S.A.S., Asnieres sur Seine, France), 3.6 µl of dH2O or CORM-2 (CO releasing molecule-2; tricarbonyldichlororuthenium (II) dimer, 100 µM final; Sigma-Aldrich, Saint Louis, MO, USA) and 20 µl of 200 mM CaCl2 as previously noted in our COHF assay [25, 27, 28]. This amount of CORM-2 increases clot strength in a standardized manner when CO is not present in detectable concentrations [25, 27, 28]. Mixtures were pipetted into disposable plastic cups in a computer-controlled thrombelastograph® (Model 5000, Haemoscope Corp., Niles, IL, USA), with CaCl<sub>2</sub> added to commence coagulation. Data were collected at 37°C for 15 min. The elastic modulus-based parameters previously described [25, 27, 28] were determined, as detailed in the legend of Fig. (1) subsequently presented.

Utilizing this technique, hypercoagulability was defined as a total thrombus generation (TTG) value >95% confidence interval value of the normal plasma data set. The presence of COHF was defined as the % increase in TTG via CORM-2 exposure that was less than the average of such measurements in normal plasma samples. For this series the value used to define COHF presence was determined to be an increase in TTG of <89%.

Iron Enhanced Coagulation Detection Assay

Plasma mixtures were composed of 320 µl of plasma, 20 µl dH2O or deferoxamine (5.6 mM final; Sigma-Aldrich) that were incubated at 37°C for 15 min in the thrombelastograph cups, before adding 20 µl of 200 mM CaCl<sub>2</sub> [27, 28]. Data were collected until the alpha value of the mixture was collected. The nonspecific decrease in MRTG value secondary to deferoxamine addition was determined by the difference in the mean between ten replicates of two conditions (without and with deferoxamine) in pooled normal plasma (George King Bio-Medical) plus two standard deviations of the deferoxamine exposed replicates – this summated to a decrease of 1.2 dynes/cm²/sec. Thus, a decrease in MRTG >1.2 dynes/cm²/sec after deferoxamine exposure would define the presence of iron mediated coagulation.
Enhancement (upper limit of normal; lower limit of normal <-0.8 dynes/cm²/sec).

**Fibrinolytic Kinetic Analyses**

Plasma samples were thawed to 37°C prior to analysis. The final mixture volume was 360 µl. The mixture was composed of 320 µl of plasma; 10 µl of tissue factor (0.1% final concentration in dH₂O; Diagnostica Stago S.A.S.), 10 µl of tissue type plasminogen activator (tPA, 580 IU/µg, Genentech, Inc., San Francisco, CA, USA; 100 IU/ml final), and 20 µl of 200 mM CaCl₂ [27, 28]. Mixtures were placed in a disposable plastic cup in a thrombelastograph® (Model 5000, Haemoscope Corp.), with CaCl₂ added as the last step. Data were collected until clot lysis time (CLT) at 37°C for was observed. Elastic modulus-based parameters of fibrinolysis were documented as previously noted [28,28], with details outlined in the legend of Fig. (2).

![Fig. (1). Effect of Alzheimer's disease on TMRTG, MRTG and TTG stratified by modulation of coagulation by CO, iron, or both.](image1)

![Fig. (2). Effect of Alzheimer's disease on TMRL, MRL and CLT stratified by modulation of fibrinolysis by CO, iron, or both.](image2)
smears were then post-fixated for 15 minutes with 1% PBS for three minutes to remove any residual fixative. The samples were then incubated for 30 minutes followed by three washing steps in 0.075 M PBS, and washed for 20 minutes. The samples were then fixated in the following in the ratios shown in Table 1, with PRP for 5 minutes. PRP smears after exposure to different compounds (see Table 1) were made on glass coverslips.

using a methodology previously noted to create extensive fibrin fiber networks, PRP smears with different compound exposures were made on glass cover slips and incubated at 37ºC for 8 minutes. A 10mM CORM-2 stock solution was prepared by mixing 1 mg CORM-2 and 195ul 100% DMSO, from hereon referred to as stock A. Stock A was used to prepare a 1mM CORM-2 solution by adding 100ul of stock A to 900ul of phosphate buffered solution (PBS), form hereon referred to as stock B. Stock B was used in the following in the ratios shown in Table 1 and incubated with PRP for 5 minutes. PRP smears after exposure to different compounds (see Table 1) were made on glass coverslips.

The cover slips were placed in 0.075 M PBS on a shaker and washed for 20 minutes. The samples were then fixed for 30 minutes followed by three washing steps in 0.075 M PBS for three minutes to remove any residual fixative. The smears were then post-fixed for 15 minutes with 1% osmium tetroxide (OsO₄), followed by a washing process, for three minutes in 0.075M PBS. The samples were finally dehydrated serially in 30%, 50%, 70%, 90% and then three times in 100% ethanol followed by drying using hexamethyldisilazane; mounting and coating with carbon. Once the samples had been coated they were analyzed with a scanning electron microscope (Zeiss ULTRA plus FEG SEM, Carl Zeiss Microscopy GmbH, Jena, Germany).

Blood was obtained from AD patients (n=12) who were diagnosed by qualified medical practitioners. All AD individuals were diagnosed using the MMSE. The AD patients were divided into 2 groups (normal and high serum ferritin concentrations, high ferritin being defined as a level of >120 ng/ml for females and >250 ng/ml for males). The AD patients did not have any chronic medical conditions, were nonsmokers, and the age of these patients was 78±12 (mean±SD) years. Fibrin fiber networks were generated as per the same methods described for healthy individuals, but without addition of iron or CORM-2.

After visualization of the fibrin networks with SEM, micrographs were obtained at 40,000 times machine magnification. A representative micrograph of each sample was selected, and subsequently a 10x5 grid was superimposed onto the picture. One fiber was randomly selected out of every block of the grid, ensuring that fiber measurements were not duplicated, and that fibers were systematically assessed to prevent observer bias [29, 30]. Fibrin fiber thickness was measured with ImageJ (ImageJ is a public domain, Java-based image processing program developed at the National Institutes of Health: http://rsbweb.nih.gov/ij/). From each sample, 50 fibers were measured.

### Statistical Analyses and Graphics

Data are presented as mean±SD, individual parameter values, % incidence with 95% confidence intervals (CI), or simply 95% CI. Coagulation and fibrinolysis parameters of AD patient samples were compared with 95% confidence intervals generated from normal plasma. A statistical program was used for student’s t-test analyses of differences in fibrin polymer fiber widths (SigmaStat 3.1, Systat Software, Inc., San Jose, CA, USA). Graphics depicting viscoelastic data were generated with a commercially available program (OrigenPro 7.5, OrigenLab Corporation, Northampton, MA, USA; CorelDRAW12, Corel Corporation, Mountain View, CA, USA).

### RESULTS

#### Viscoelastic Analyses

Eleven AD patients (7 male), aged 73±10 years, with MMSE values of 20±3 and body mass index (BMI) values of 24±3 kg/m² were recruited. In regard to comorbidities, no patient had diabetes mellitus, one had a history of migraine, one had a history of myocardial infarction, four had hypertension, and one had a history of asthma. We had originally requested 10 patients to study, but an additional patient had blood collected, so the vendor was kind enough to donate the plasma and clinical information of this patient for our study.

As for normal plasma values, the 95% confidence interval values for coagulation and fibrinolytic parameters are depicted in Table 2. For an AD patient to be considered hyper/hypocoagulable or hyper/hypofibrinolytic, the kinetic parameter value of interest had to be outside the normal 95% CI values. The criteria for COHF formation and iron enhancement of coagulation was presented in the materials and methods section previously.

Fig. (1) displays the coagulation profiles of the AD patients stratified by COHF formation (CO enhancement of coagulation), enhancement of coagulation by iron, or
enhancement of coagulation by both CO and iron. Of interest, there was no patient without modulation of coagulation by either CO or iron. With regard to CO, ten of eleven patients had COHF formation, whereas seven patients had iron enhanced coagulation kinetics. With regards to TMRTG, one patient had a hypocoagulable TMRTG value, two patients had hypercoagulable TMRTG values, with the remainder within the normal range. As for MRTG, seven patients had hypercoagulable values, two patients had values exactly at the 95% CI value of normal, with the balance being within the normal range. In the case of TTG, five patients had abnormally strong thrombi, with the balance being within the normal range.

**Table 2. Normal 95% CI values for coagulation and fibrinolytic kinetic parameters.**

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Values</th>
</tr>
</thead>
<tbody>
<tr>
<td>TMRTG (min)</td>
<td>2.6-4.3</td>
</tr>
<tr>
<td>MRTG (dynes/cm²/sec)</td>
<td>3.8-8.9</td>
</tr>
<tr>
<td>TTG (dynes/cm²)</td>
<td>127-237</td>
</tr>
<tr>
<td>TMRL (min)</td>
<td>3.6-24.9</td>
</tr>
<tr>
<td>MRL (dynes/cm²/sec)</td>
<td>0.6-1.4</td>
</tr>
<tr>
<td>CLT (min)</td>
<td>13.0-34.5</td>
</tr>
</tbody>
</table>

Time to maximum rate of thrombus generation (TMRTG): this is the time interval (min) observed prior to maximum speed of clot growth; Maximum rate of thrombus generation (MRTG): this is the maximum velocity of clot growth observed (dynes/cm²/sec); Total thrombus generation (TTG): this is the total area under the velocity curve during clot growth (dynes/cm²), representing the amount of clot strength generated during clot growth; time to maximum rate of lysis (TMRL): defined as the time when maximum amplitude is observed until the time (min) of maximum velocity of clot lysis is observed; maximum rate of lysis (MRL): the greatest velocity of clot lysis (dynes/cm²/sec); CLT: defined as the time (min) from when growth ceases until lysis is complete (amplitude returns to 2 mm).

Fig. (3). Healthy fibrin fiber network. Plasma with thrombin added to create an extensive fibrin network is depicted. Ten ul of plasma was added to 5 ul thrombin (10 U/ml human thrombin in ddH2O), mixed and incubated for 3 minutes to create an extensive fibrin network. Individual fibrin fibers are visible. A typical 5 by 10 grid was superimposed, which was used to assess fibrin fiber diameter as discussed in text. Scale bar = 1 μm.

Fig. (2) displays the fibrinolysis profile data of AD patients stratified as seen in Fig. (1). With regard to onset of clot lysis, all AD patients had normal TMRL values. However, four AD patients had an above normal increase in MRL values, indicating an increased vulnerability to lysis, while the remainder of the group had values in the normal range. Lastly, only two of the eleven AD patients had CLT values that were below normal values, indicative of a hyperfibrinolytic tendency in these individuals.

**SEM-Based Analyses**

The AD cohort from the University of Pretoria was composed of ten women and two men; the normal ferritin group had a serum ferritin concentration of 66±33 ng/ml whereas the high ferritin group had a significantly (P=0.0003) ferritin concentration of 253±88 ng/ml.

With regard to SEM data, Fig. (3) shows a typical, normal subject fibrin network with mostly major, thick fibrin fibers. In healthy individuals, individual fibrin fibers are visible, appearing like a net, with no fused fibers and no fine, lattice-like appearance. When FeCl₃ is added to PRP followed by exposure to thrombin, (Fig. 4A) a finer fiber lattice net is observed (see thick white arrow), as well as areas forming a denser mesh (see *), where the lattice net fuses to form a matted deposit. Close examination revealed areas of denser fibrin deposits (*), consisting of fine fibers (see thin white arrow) that were packed closely to each other.

Addition of CORM-2 to PRP, followed by exposure to thrombin, resulted in fibrin fiber diameters that were also decreased compared to the healthy fibers but were more densely packed, with a more globular structure compared to the rather straight individual fibers seen in the healthy fibrin structure (Fig. 4B). This ultrastructure was suggestive of CORM-2 modifying the fibrin packaging. Fig. (5A and B) compared high magnification healthy fibrin fibers to that of healthy PRP exposed to CORM-2.

Fig. (6A-F) shows fibrin networks from the individual AD patients with normal serum ferritin levels. Here we see that the fiber diameter increases. Fig. (7A-F) shows fibrin networks of Alzheimer’s patients with high serum ferritin levels. The fibrin fiber nets resemble that seen in Fig. (4A) (FeCl₃ is added to PRP followed by thrombin exposure), where the net resembles a fine lattice. We also noted that the individual fibrin fibers of both the normal and high serum ferritin AD individuals showed a more globular morphology, as seen with CORM-2, instead of the rather straight and smooth individual fibers seen in the healthy subject fibrin fibers. See arrows indicating globular structure in Fig. (6 and 7).

With regard to average fibrin fiber width, the value for the normal subjects was 105±3 nm. Exposure to FeCl₃ decreased fiber width by 58% and exposure to CORM-2 decreased width by 43%. The average width values for the AD patients, stratified by serum ferritin concentration, are depicted in Fig. (8). The high ferritin AD group had a fiber width that was significantly less than the normal ferritin AD group, with an average value 34% less than the high ferritin group.
Fig. (4). Healthy fibrin fiber network with added FeCl₃ (A) and CORM-2 (B) and thrombin to create an extensive fibrin network. (A) 10 ul PRP was added to 5 ul FeCl₃ (1mM) and mixed followed by addition of 5 ul of thrombin; this was mixed again and incubated 3 min. Thick arrow (left) - fine fiber lattice net; * - areas of denser fibrin deposits, consisting of fine fibers (see thin arrow (right)) that are only packed closer to each other. (B) 10 ul of stock B CORM-2 was added to 990ul PRP (see table 1 for CORM-2 preparation); then 20 ul of PRP was exposed to CORM-2 followed by addition of 10 ul thrombin; this was mixed and incubated for 3 minutes. Globular fibrin packaging is visible, without typical straight fibrin fibers seen in healthy fibrin nets. Scale bar = 1 μm.

Fig. (5). High machine magnification (100,000x machine magnification) of healthy fibrin fiber network (A) and with added CORM-2 (B) and thrombin to create an extensive fibrin network. Preparation as described in figure 4. Arrows show smooth and straight fibrin fiber packaging in (A) and globular fibrin fiber structure in (B). Scale bar = 100 nm.

Fig. (6). Contd…
Fig. (6). Fibrin fiber networks of six AD patients (A-F) with normal serum ferritin levels. Ten ul of AD plasma was added to 5 ul thrombin (10 U/ml human thrombin in ddH₂O), mixed and incubated for 3 minutes to create an extensive fibrin network. Healthy values for ferritin are 20 to 250 ng/ml for males and 10 to 120 ng/mL for females. Globular areas, similar to that observed with CORM-2 exposure are indicated with arrows. Thus, more of a CO effect on fibrin polymer formation is likely. Scale bar = 1 µm.

Fig. (7). Fibrin fiber networks of six AD patients (A-F) with high serum ferritin levels. Ten ul of AD plasma was added to 5 ul thrombin (10 U/ml human thrombin in ddH₂O), mixed and incubated for 3 minutes to create an extensive fibrin network. Globular areas, similar to that observed with CORM-2 exposure are indicated with arrows. Unlike patients' clots in figure 6, both fine fiber lattice and globular areas are present, consistent with a combination of iron and CO mediated changes in fibrin polymer formation. Scale bar = 1 µm.
DISCUSSION

The most prominent observations of the present investigation include the finding that all patients afflicted with AD evaluated with viscoelastic methods had modulation of plasmatic coagulation by CO, iron, or both. Of equal and critical importance, the ultrastructure of plasma clots obtained from AD patients displayed morphological features consistent with both iron and CO exposure, similar to normal plasma exposed to FeCl₃ and CORM-2. We further stratified the AD patients by plasma ferritin concentration, not just for being at risk of exposure to greater circulating iron concentrations but also as an indirect marker of increased Hmox activity as has been demonstrated previously [31,32]. Thus, the significantly smaller fibrin fiber diameter observed in AD patients with high serum ferritin levels very well may be secondary to increased iron and CO secondary to more pronounced cerebral Hmox activity (Fig. 8). In sum, the coagulation kinetic and ultrastructural data support the concept of exposure of the circulation to increased concentrations of iron and CO, and given the relative absence of confounding comorbidity in both cohorts of AD patients, the most likely source of iron and CO was AD associated, increased cerebral Hmox activity.

In contrast to the aforementioned coagulation and ultrastructural data, the observation that most of the AD patients undergoing viscoelastic analyses had normal to increased vulnerability to tPA mediated lysis was an unexpected finding (Fig. 2). Indeed, four patients had abnormally great rates of clot lysis and two had abnormally decreased clot lysis times. It would be expected that increased CO and iron would attenuated fibrinolysis in the absence of any other biochemical aberration [17]. Thus, the data of the present investigation support the concept that an endogenous fibrinolysin may have been present despite increased Hmox activity, as has been documented by us in the settings of obesity and cancer [33, 34].

When our data are considered as a whole, CO and iron enhanced coagulation could play a role in spontaneous cerebral embolus formation in the setting of AD as documented by previous ultrasonic investigations [11, 12]. Further, when coupled with normal or accelerated fibrinolysis, it is possible that microembolic or in situ thrombus formation within the brain occurs causing ischemic damage, but with timely lysis preventing large, clinically detectable neurologic defects. Nevertheless, over a period of years, it is possible that such a pathological state of coupled microischemic stroke/fibrinolysis could eventually result in minimal cognitive impairment and ultimately AD. The notion that inhibition of Hmox chronically could perhaps greatly delay the onset of AD is borne out in experiments with transgenic mice that mimic AD, as both behavioral and neuroanatomical changes that occurred over time were prevented with Hmox inhibition [24]. In sum, only human studies using this therapeutic approach, perhaps at first in those with minimal cognitive defect, will help define the part played by Hmox and the specific mechanism(s) by which Hmox contributes to AD.

While promising, the data of the present investigation serve primarily as a “proof-of-concept” of the involvement of CO and iron interactions with the circulation as a possible contributor to AD. Utilizing our analytical methods to correlate CO and iron mediated modulation of coagulation and plasmatic hypercoagulability with clinical progression of dementia in critical long term studies remains to be performed. If increased cerebral Hmox activity plays a role in the progression of dementia [18-21], then our hematological methodology might be utilized to correlate changes in coagulation with changes in brain pathology (e.g., tissue iron deposition). Thus, if novel therapeutic innovations (e.g., Hmox inhibition, iron chelation) are tested clinically to slow or abrogate dementia, the efficacy of such interventions can be assessed with simultaneous clinical assessment, magnetic resonance imaging, and viscoelastic/ultrastructural analyses. At a minimum, we plan to establish such correlations with progression of disease in future investigations.

In conclusion, our study demonstrated that two small cohorts of AD patients had viscoelastic and ultrastructural evidence of CO and iron modulation of coagulation. Further, hypercoagulability was observed, with velocity of clot growth the most prominent feature – and iron and CO both increase clot growth velocity [17]. This enhancement of coagulation was coupled with normal to enhanced vulnerability to lysis, perhaps significantly contributing to ephemeral microembolic phenomena that only over time result in clinical dementia. Future study of the part played by Hmox-generated CO and iron in the pathogenesis of dementia and concurrent hypercoagulability is warranted.

CONFLICT OF INTEREST

The authors confirm that this article content has no conflict of interest.
ACKNOWLEDGEMENTS

This investigation was supported by the Departments of Anesthesiology and Physiology.

REFERENCES


